



LUCAS FIORINI BRAGA

**CONTROLE DE AMBIENTES INTELIGENTES
POR COMANDOS MENTAIS USANDO EEG**

LAVRAS – MG

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Monografia apresentada à Universidade Federal de Lavras, como parte das exigências do curso de Ciência da Computação, para a obtenção do título de Bacharel.

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Orientador

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Dedico este trabalho aos meus queridos pais Roberto Alves Braga Júnior e Vanessa Mesquita Braga, meus avós Délcio Mesquita, Celma Maria Mesquita, Roberto Alves Braga e Dorothy Aparecida de Souza Braga.

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RESUMO

O último Censo Brasileiro revelou que o número de pessoas com deficiência física no Brasil em 2010 girava em torno de 6,7 % da população. A interação cérebro-computador com sensores de eletroencefalograma tem mostrado bom potencial para permitir a interação de pessoas com deficiências que limitam seus movimentos e capacidade de controlar dispositivos interativos. Este estudo teve como foco um estudo exploratório para investigar a usabilidade de um equipamento baseado no reconhecimento de abstrações mentais, usando um eletroencefalograma sem fio para controlar um ambiente doméstico inteligente. As avaliações envolveram 30 estudantes brasileiros sem deficiência física ou intelectual diagnosticada, como um primeiro estudo para investigar a usabilidade da abordagem, precedendo testes futuros com pessoas com deficiência física. Este estudo teve como objetivo analisar a usabilidade de uma abordagem em que comandos mentais manipulam um bloco virtual como proxy para o controle de eletrodomésticos. O método incluiu a análise de problemas de usabilidade, precisão, dificuldade da tarefa, satisfação e reações emocionais durante as tarefas. Os participantes do estudo mostraram um alto nível de aceitação em relação à dificuldade e precisão. O estudo também revelou várias limitações do hardware, sendo sua especificidade de usuários ótimos, como pessoas com menos ou mais cabelos finos e a delicadeza dos eletrodos. Com os resultados, pudemos identificar como grande parte das variáveis interfere nas métricas e o impacto positivo na comunidade de acessibilidade.

Palavras-chave: EEG; Eletroencefalografia; Casas Inteligentes; Acessibilidade; Usabilidade

Article

Usage of EEG for mental commands at home assisted environments

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Abstract: Brain-computer interaction with electroencephalogram sensors has shown good potential to enable interaction for people with disabilities that limit their movements and ability to control interactive devices. This study focused on an exploratory research to investigate the usability of an application based on recognition of mental abstractions, using a wireless electroencephalogram to control a smart home environment. Evaluations involved 30 Brazilian students with no physical disabilities diagnosed, as a first study to investigate the usability of the approach, preceding future tests with people with physical disabilities. This study aimed to analyse the usability of an approach in which mental commands manipulated a virtual block as a proxy to control house appliances. The method included analysing usability problems, accuracy, task difficulty, satisfaction and emotional reactions during the tasks. Study participants showed a high acceptance level concerning difficulty and precision. The study also revealed several limitations of the hardware, being its specificity of optimal users like people with less or thinner hair and the delicacy of the electrodes. With the results, we were able to identify how most of the variables interfere in the metrics and the positive impact on the accessibility community.

Keywords: EEG; Smart Home; Assistive Technology; Usability; Electroencephalography;

1. Introduction

Advances in Internet of things (IoT) technologies have boosted the availability of technological solutions to support activities in people's daily lives. Among these technologies are the Ambient Assisted Living (AAL) systems and Smart Homes [2]. Smart homes seek to automate everyday tasks to provide facilities for domestic activities [11]. Among the tasks that this technology can perform is the control with more ease of equipment, features, and appliances present in the environment.

AAL systems seek to support older people and people with physical disabilities in their daily routine. Its main objective is to promote autonomy and security in these people's daily lives in the domestic environment [7]. These systems are often composed of several sensors to monitor users present in the environment and offer medical care remotely [16].

For the control of smart homes and AAL systems, there are various modes of interaction in the area [21]. The use of voice commands and intelligent sensors allow the user to interact with the system. This diversity of interaction modes enable different types of users to take advantage of smart home technologies, including people with different kinds of disability. However, the main focus is disabilities such as quadriplegics, paraplegics or people with similar injuries. For example, this group of people may find it more suitable to use interactions by voice commands to perform tasks in the home environment more efficiently (such as turning on lights, turning on appliances, among others) [5]. Thus, the use of AAL systems proves to impact accessibility, autonomy, and independence significantly for people with different levels of limitations [25]. These characteristics are essential for the quality of life of these users [5].

36 Even though these technologies provide significant assistance, people with motor disabilities may
37 have many more complicated challenges dealing with how they interact with their home environment.
38 For example, in more severe cases, people who are paraplegic or quadriplegic may need different
39 interaction mechanisms, such as eye-tracking[22] and brain-computer interaction [15].

40 Mental commands as data entry for systems are a fundamental approach to allow interaction. The
41 use of this mode of interaction is very present in assistive technologies for people with motor disabilities.
42 A good example is the research of wheelchairs controlled by mental commands [13, 20, 10]. By mapping
43 brain signals, it is possible to assign an action to be performed by the equipment/system/technology
44 in question.

45 The application of mental commands for the control of smart homes by people with motor
46 disabilities is another solution to give autonomy and independence to these people in the home
47 environment.

48 This study aimed to analyze the usability of an approach in which mental commands manipulated
49 a virtual block as a proxy to control house appliances. The method included analyzing usability
50 problems, accuracy, task difficulty, satisfaction and emotional reactions during the tasks. As the
51 versatility of electroencephalography is paired with many doubts about being intrusive or invasive,
52 this study brings metrics obtained through assessments and detailed video analysis which reinforces
53 not only the technical issues found but also the usability perceived by the users.

54 The remainder of this paper is organized as follows. Section 2 presents the main concepts related
55 to Brain-Computer Interaction, Smart homes and Ambient Assisted Living and related work. Section 3
56 presents the main methodological aspects. Section 4 presents the results obtained, which are discussed
57 in Section 5. Finally, Section 6 presents conclusions and future work.

58 2. Theoretical Background

59 2.1. Brain-Computer Interaction (BCI)

60 Brain-computer interfaces (BCI) refer to a technology aimed mainly to aid the communication
61 and independence for neuromuscular impairments via the electrical potential information from the
62 brain[28]. This potential that is further translated to usable information, is acquired at the cortex of
63 the brain, the closest layer from the scalp. BCI have had significant growth in research interest. This
64 type of interface corresponds to systems that incorporate algorithms that translate input from users
65 into commands to control devices [28]. Electroencephalography has been widely used to enable BCI,
66 and it is evolving with more sophisticated models, causing it to be widely used across medicine.

67 As described by Lin *et al.* [14], (EEG) equipment is a powerful tool for capturing and
68 understanding the multiple variations of cognitive states of its users without the need to maintain the
69 head in a fixed state, being able to give researchers valuable data like feelings, alertness and attention
70 [8]. That is mainly due to its non-invasive and non-intrusive properties provided by attributes like
71 the lack of wires for using a battery, lightweight, and facility to wear. This brain-imaging equipment
72 functions by placing electrodes over some strategic regions of the scalp, calculating the electrical
73 potential generated by these areas. A measurement of an electrical pulse derived from a dense mass
74 of neurons can only measure the information from this area and not from individual neurons. This
75 process is also exposed by the interference caused by the different conductivity of surrounding tissues
76 between the neurons and the electrode [17]. Some studies like [29] and [24] work on signal processing
77 algorithms to predict and classify the patterns.

78 The signal quality and accuracy measured when there is a change in mental state, response to
79 internal or external stimuli and directed attention can be attenuated not only by physical barriers. For
80 example, eyes opened or closed can lead to different values caused by visual input [3]. Personal traits
81 from each individual and the current state during its use (level of attention and amount of external
82 interference) can make the task of providing a reliable solution even more delicate. So the biggest

83 challenge, according to Mihajlovi *et al.* [17], is finding a solution smart enough that provide a superior
84 signal quality and, at the same time, a comfortable and convenient for the user.

85 This technology can be found more consistently in hospitals for predicting epilepsy occurrence
86 [18] and even understanding better the brain recovery after traumas or procedures. This equipment is
87 also found in clinics that perform exams such as polysomnography. However, the process of installing
88 EEG equipment may be cumbersome for users. They need to go through a skin-clearing which involves
89 sometimes abrading it, followed by gel application used for sticking the electrodes and also increases
90 the current flow between the equipment and the user's head [27]. All these procedures make the
91 process intolerable and uncomfortable for the user, leading to biased and noisy results, bearing the
92 need for equipment with better overall usability.

93 2.2. Smart homes and Ambient Assisted Living

94 With a low cost and a wide variety of ways to control an intelligent environment, smart houses
95 are have attracted increased research attention. Some authors may describe it as a house that can
96 capture information, control its appliances and also be flexible enough to fit several ways of controlling
97 it[2]. What makes it possible is a noticeable growth on the Internet of Things (IoT) field. It allows a
98 cost-effective way to exchange information and interconnect equipment to share information and to
99 work simultaneously. It is more feasible to assemble an Ambient Assisted Living (AAL) that suits
100 multiple disabilities in this given context.

101 Those types of Smart Homes can offer, with particular ease and precision, ways to control it
102 that covers many physical impairments. For example, Bempong [12] discusses ways to modify a
103 smart ambient in ways that it notifies deaf and hard-of-hearing users when it produces a sound.
104 Oliveira *et al.* [19] in other hand produced, by screen-reading technology, a method that aid people
105 with vision-related disability to be able to control its environment. Another inclusive mechanism for
106 special needs would be electroencephalography-based control. This one can support serious motor
107 disability users to be more independent when controlling their surroundings, such as interacting with
108 the television and turning on or off other home appliances.

109 2.3. Related Work

110 The usage of EEG equipment can bring a layer of ease when it comes to task automation for
111 complex mechanical disabilities. Architectures that involve EEG signal processing for this purpose are
112 more widely available, with the widespread use of IoT technology. Partha *et al.* [24] used the Emotiv
113 EPOC+ to obtain brain signals and try to use predictive models to extract information from them. This
114 study tries to use this method mentioned above to turn on and off a light bulb.

115 The same type of study was conducted by Wenchang[29] who also worked at the back-end part
116 acquiring and processing data with artificial intelligence methods from EEG signals. Moreover, when
117 it comes to home automation targeting disabled people, the studies focus on approaches that still
118 require the user to leave its physiological state to interact with it. At this point, studies like the ones
119 performed at [14] or [15] target the house interaction with the lowest effort possible mainly because
120 of the designated audience composed of elderly people or severely disabled people. In the study
121 conducted by Luo *et al.* [15], the EEG chosen was the same as this study, the Emotiv EPOC. Differently
122 from the studies that deal with back-end signal processing. Here was opted to use the processing
123 system developed by Emotiv's company themselves and translated the acquired signals to the house
124 commands. Another study that addressed the life quality and greater independence for people with
125 severe physical problems using BCI was Ullah [26]. The goal was to build a single-channel EEG with
126 self-made electrodes and produce a tool for communication with no need for physical interaction.
127 Aiming at low costs and easy setup, the software aid the communication for those targets via SMS and
128 got an 87% rate of accurate typing.

129 Other usages of BCI can be contemplated by Rebsamen [23] and Craig [6], who developed a
130 mental command-based system to manipulate a wheelchair. Another example can be the usage of
131 EPOC embedded gyroscope to control a robotic arm proposed by [1]

132 Partha *et al.* [24] proposed an in-depth study on the BCI field for home automation while
133 focusing on testing a custom-made machine learning model described as a combination between Long
134 Short-Term Memory (LSTM) and classical Random Forest Classifier (RFC), and also discuss the data
135 retrieved from different areas of the brain. Using a commercial solution, the EPOC+ was the EEG
136 solution to gather data for future usage into the classification methods. Hereafter, the testing procedure
137 was conducted in two phases using eighteen healthy users with 20 to 25 years old with no records
138 informed about the existence of prior knowledge about EEG systems. The final intention was to test
139 the accuracy of the classification method aforementioned in acting on turning on and off a lamp.

140 The test setup was conducted under the following circumstances, a well-lit and quiet room where
141 the instructions were given through audio and video from a computer there placed. The first phase
142 consisted of showing an image of a glowing bulb and asking the subject to give mental commands for 14
143 seconds to turn it off while limiting the body movement and maintaining the eyes closed. After that, in
144 the second phase, the user maintained a relaxed state of mind with the equipment still recording for 15
145 seconds to represent the *no-command* state, then repeated the training for turning on the bulb. With the
146 data acquired, it went through denoising, digital filter, cleaning, and a parameter-based pre-processing
147 to be feed into the hybrid model proposed. With no possibility of interaction with the image and any
148 user feedback presented, it was not possible to track the emotions and the user-perceived precision.

149 Finally, to calculate its efficiency, no questionnaires focused on user experience. Therefore, there
150 were no data on difficulty or emotional reactions. Instead, the data acquired was used to train, validate
151 and test the model accuracy. The proposed model performed better than a Support Vector Machine
152 used for comparison reasons, and, using the optimal electrode setup, its accuracy was 68.36%. After
153 all, the limitations concentrated on discovering more detailed information about the behavior of some
154 regions of the brain and a better method of gathering features with more precision.

155 Another solution for smart home automation with BCI was designed by Luo *et al.* [15]. Here,
156 the equipment was the same as the previous one, Emotiv EPOC+ and there was also developed an
157 Android system to enhance the accuracy of control. Unlike many previous papers mentioned, in this
158 study, the signal was not processed in a custom way. The data acquired from the users was processed
159 by the Emotiv software itself and sent the results to a control unit. After passing the control unit, the
160 micro-controller unit (MCU) coordinates environmental objects such as TV, air-conditioning, curtain,
161 door, and light. The study counted with five users being two of them already familiarized with the
162 technology, average age of 21 years old, two females, and no further information on special physical
163 needs. The environment had no declared condition pattern for the tests and no specification on how the
164 users performed the training. The tests involved six actions, turning on and off air-conditioning, light
165 and opening and closing curtain, and for each one, the recording occurred five times. The accuracy
166 metric was related to the Up command, which is to move the block upwards at the Emotiv Control
167 Panel software. Therefore, the success rate was the number of successful attempts to control a subject
168 divided by the total attempts. No information about the user experience was obtained, neither the
169 overall emotional reactions related to the actions performed. There were two rounds of tests, the first
170 one without the Android software to control the command stability and the second one. The first
171 one got an average accuracy of 29.6%, being the lowest 13.33% and the highest 33.33%. Now with
172 the Android software, the results raised to 84%. Barriers encountered by this study were the lack of
173 stability of the EEG signals, transmission delay, chock in communication among some parts, and the
174 memory overflow at the central control system.

175 Like aforementioned, the studies covers mainly the technical aspect related to EEG usage and
176 application. Also, at some of them, the main focus was to identify an accurate model to classify the
177 information gathered by EEG. In other hand, other researches focused on building cheap equipment
178 or to integrate it into other solutions instead of home usage. But, the main problems when, it comes

179 to EEG solutions, are the usability aspects. This is why this study gave a lot of attention for this part,
180 which as missing in the literature and is so important.

181 3. Method

182 3.1. Study design

183 The study aimed to perform a usability evaluation of a smart home resource control prototype
184 with control by mental commands and facial movements, evaluating the reactions and user experience
185 with the commands.

186 For the usability evaluation, an intra-participant design was chosen so that all participants will
187 be exposed to the test conditions with a set of mental commands and facial movements for a series
188 of actions to be carried out on the smart home prototype, operating a TV and a lighting system. The
189 movements and commands chosen were defined through a previous analysis whose objective was to
190 select those that require less effort.

191 After each action, participants assigned ratings for aspects measured by the Self Assessment
192 Manikin - SAM [4], with variables of satisfaction, motivation, and feeling of control. Also, participants
193 were asked to complete a questionnaire on the use of technologies and demographic data.

194 Before each evaluation, users were informed about the research objective, in addition to the
195 privacy policies for the use of data and the analysis and publication of results.

196 Participants were completely voluntary and could withdraw participation at any time during the
197 evaluations. The university's Research Ethics Committee approved the usability assessment protocol
198 with id: CAAE 66819517.3.0000.5148. All participants signed a consent form authorizing the collection
199 and use of data.

200 3.2. Application evaluated

201 To develop an interface between the Smart Environment and the electroencephalogram, the EEG
202 tool was first chosen. The Emotiv EPOC+ is a model that counts on fourteen channels for complete
203 brain sensing. The fourteen channels used to retrieve data using the sequential sampling method are
204 AF3, F7, F3, FC5, T7, P7, O1, O2, P8, T8, FC6, F4, F8, AF4, as shown in Figure 1. It uses a saline-based
205 compound to connect the electrode over the scalp better, enhancing the signal retrieved by the electrical
206 potential at these areas. This model connects via Bluetooth, which increases mobility and supports the
207 non-invasive and non-intrusive principles. Another favorable feature brought by this model is the
208 ease to install it over the user's head due to a mild amount of connectors and lack of wires, making the
209 setup faster and less meddling.

210 The software that comes with the drivers and enables several interfaces to interact with its
211 functionalities, called Emotiv Xavier Control Panel v3.5.1, can help the user identify if the electrodes
212 are correctly positioned and working appropriately. After the setup, which also includes a user profile
213 that saves training progress, the used areas for this study were only the Facial Expression and the
214 Mental Command sections. Other functions like Performance Metrics that measure specific emotions
215 and Inertial Sensors that detect head movements were not used in this study.

216 With the EEG ready, there was a code integration between two sources. The first one, no longer
217 available, was the EPOC+ developer Java code made available by Emotiv developers. The second code
218 part was obtained by previous studies on Assistive Homes found at [19]. As described in Figure 2, the
219 EPOC+ Figure 2 (3) was connected via Bluetooth with the computer Figure 2 (4) was the application
220 caught the information received by this equipment, translated that mental command input to the
221 mapped action associated with it and sent it over an MQTT(Message Queuing Telemetry Transport)
222 protocol. Once the server subscribed to that topic, a micro-controller like Arduino or Raspberry Pi
223 Figure 2 (8) would receive the information and translate it to events at the environment connected to it,
224 for example, turn on or off the TV Figure 2 (9).

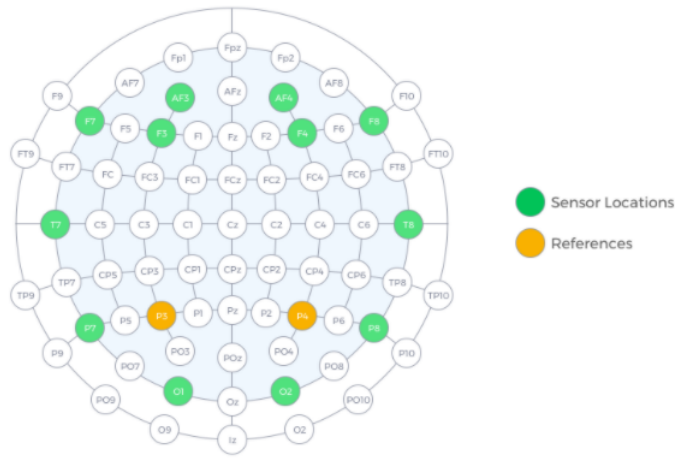


Figure 1. Emotiv EPOC+ connection points [9]

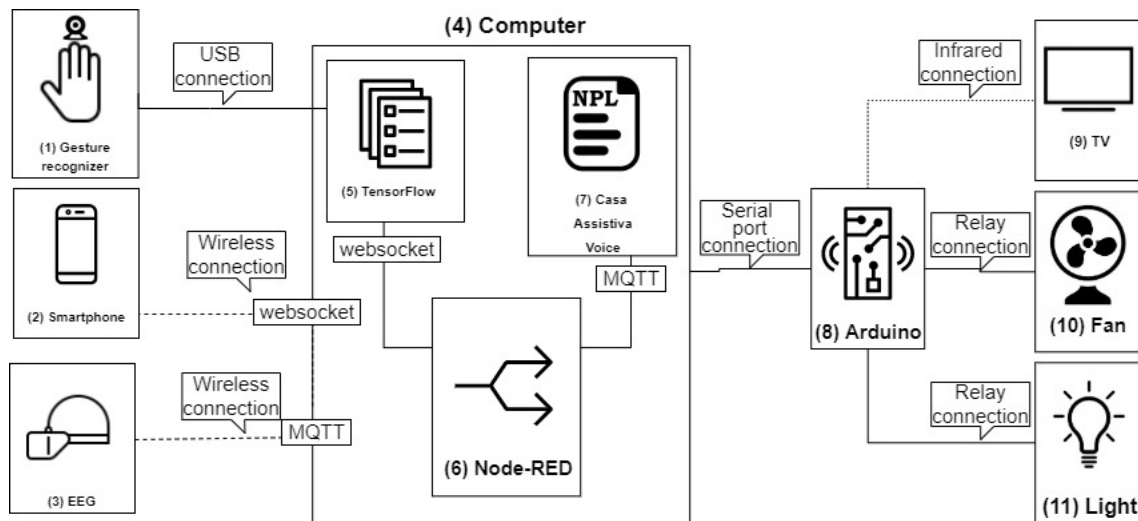


Figure 2. Smart House Architecture (OLIVEIRA 2020)

225 The possible signals received from the electroencephalography equipment were the PUSH, LIFT,
 226 and SMILE. The first one was a task based on pushing a virtual block to the end of the scenario Figure
 227 3. It was translated into a turning the TV command Table 1. The second was relatively the same
 228 as the first one, but the command was lifting the block, which was translated to changing the TV's
 229 channel. Finally, the third captured the smile facial expression made by the user. This command would
 230 represent turning off the TV.

Command	Code	Action
Smile	T1	Turn TV Off
Lift	T2	Change TV Channel
Push	T3	Turn TV On

Table 1. Mental command mapping

231 The choice of translating those signals from mental commands to actual actions in the smart
232 environment was to mitigate the complexity of thinking about such abstract commands. Turning on
233 television is a simple task, but it is not as easy to materialize its action mentally as pushing a virtual
234 block. This approach saved time during the testing, which is a significant matter for performing a
235 less invasive and tiring process to the user, and helped improve the overall accuracy of the tasks by
236 making them think only about the block in front of them.

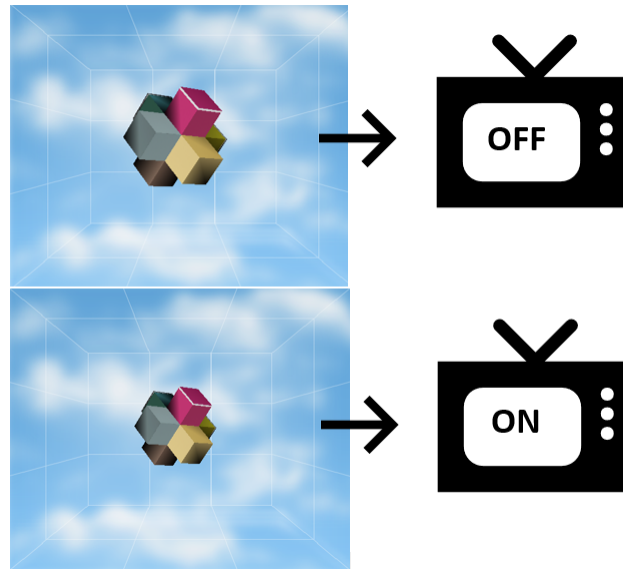


Figure 3. Emotiv Xavier 3.5.1 mapping to assistive home command

237 3.3. Evaluation Procedures

238 The procedure started by explaining to the user the primary motivation of the study and how
239 the equipment works. Further on, the test moderator explained the privacy policies for using their
240 image only by the researchers and the possibility of giving up at any given time due to excessive
241 discomfort. After setting the system up and ready to start, the user was asked to follow the Think
242 Aloud protocol during the whole experiment. Therefore, it would enable the researchers to re-watch
243 the tests and comprehend in-depth details that could not be noticed first. That step also improves
244 the ability to understand the cognitive process used by the users. Meanwhile, the video was also
245 recorded to identify facial expressions that could lead to discomfort, excitement, confusion, or other
246 traits of feelings that could emerge. After those statements were clear, the main focus was to clarify
247 how the test would be conducted before it got started. This way, there would be no interference on the
248 recording.

249 After the setup and preliminary explanations, the user was asked to focus as much as possible on
250 a neutral mental state where he/she was supposed to think about nothing or to focus on a certain spot
251 to prevent any sort of distraction for thirty seconds. At this moment, the participants often tended
252 to do it with their eyes closed, which showed a significant increase in the precision of this type of
253 command. Afterwards, three more neutral state training exercises were performed to increase the
254 accuracy captured by the equipment. The moderator made it clear that at these, they were supposed to
255 perform the same focus routine as they performed at the thirty seconds one to maintain the consistency.
256 When the neutral training was over, the same was executed with the other two actions. One of them
257 was to concentrate on lifting a block that appeared on the screen for seven seconds and the other
258 on pushing that block forward. Both of them needed at least four iterations to achieve a significant
259 accuracy (above seventy per cent).

260 The actions performed were guided by the software, where the block moved, so the user could
261 better understand how it should move and give them better confidence. Therefore, after all, training
262 steps were finished, the system started to run, and meanwhile, he was asked to stay in a neutral state
263 and as soon as the tester asked to perform one of the actions previously seen, the software should
264 capture it and translate to one of the house tasks such as turn on the TV for the mental command push
265 and next channel for the lift action.

266 Tests aimed at evaluating mental commands and one command based on facial expressions to
267 turn off the TV in the assistive environment. In this case, the expression was the smile. For this phase,
268 similar to the previous one, a neutral facial expression was captured for thirty seconds and three more
269 times for seven seconds, Figure 4. Later on, the smile expression was captured at least three times to
270 get the desired precision to be able to go on to the test on the actual smart house.

271 Finally, the evaluation of each task also had a score assigned by participants from one to nine to
272 rate their satisfaction, motivation, and feeling of control. Before answering the questions, the moderator
273 explained that satisfaction was supposed to be evaluated considering how challenging the tasks were
274 and how complicated it was to understand. For motivation, participants should also consider the
275 mental overload throughout the test, and a feeling of control was referred to as the perceived accuracy.



Figure 4. User performing neutral facial expression training

276 3.4. Participants

277 The study recruited participants who were undergraduate university students from any course
278 with no intellectual or physical disabilities, considering that the study was a pilot evaluation to assess
279 the mental commands' usability before the actual evaluation with disabled users. The metrics obtained
280 would be less likely to have any noise derived from these conditions and represent more precisely the
281 conditions observed from the equipment.

282 3.5. Data Analysis

283 The analysis involved a content analysis, which involved watching the videos produced to extract
284 details of the sessions, including usability problems and emotional reactions. Among those details,
285 it can be pointed facial expressions of traces of feelings like excitement or confusion. The amount of

286 training required for each task, its precision, the level of confidence noticed, and other variables that
287 could be interfering were noted to be evaluated.

288 We also observed whether the eyes were open or closed during the whole time or partly. This
289 factor was observed in another study conducted by Barry *et al.* [3]. This detail can change the precision
290 of the task completely, being important to note.

291 The next step was to require the user to evaluate each task. Participants rated each task on scales
292 from one to nine on the level of confidence, the feeling of control, and the motivation scores. These data
293 were cross-tabulated with the videos' data and related the events observed with the scores pointed.

294 4. Results

295 4.1. Participants profile

296 The thirty participants were graduating students with no restriction on which course and with
297 no physical disabilities. The mean age of the participants was around 22 years old (Figure 5), and
298 the majority were men due to a problem encountered while testing with women. Such a problem
299 happened due to a poor or absence of connection between the scalp and the electrodes.

300 To avoid biased results, all the users did not know how the EEG worked and never used this
301 sort of technology before. That circumstance supports the theory that any person with no previous
302 background in that technology category can come up with good results out of its usage.

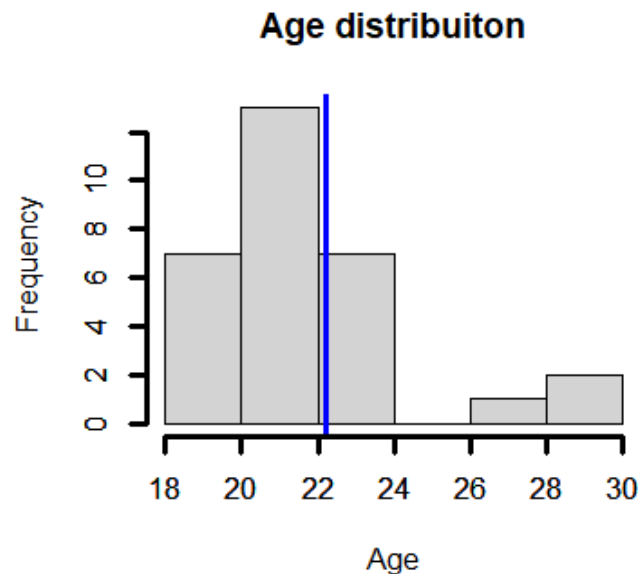


Figure 5. Participants age distribution

303 4.2. Usability problems encountered

304 One of the main problems with the EEG was the fragility of its sensors. Massive maintenance
305 was required to keep them plugged correctly at the helmet structure without a thick layer of oxidation
306 under the hydrated sponge that prevented the electrical signals from flowing correctly. Another
307 significant barrier to the test was the amount of hair. The user could not have a thicker hair type
308 because it would make the headset unable to connect correctly, leaving a poor connection of less than
309 half of the electrodes or even no connection at all. That issue also propagated to female participants
310 due to its considerable likelihood of having a longer and thicker hair layer between the scalp and the
311 electrode sponge.

312 Before the usability test was carried out, many tests were performed with the EEG. A significant
 313 threat to the complexity and duration of the test was with joining two or even more commands together
 314 at one single user profile. That user profile is a form that Emotiv Xavier uses to separate user training
 315 info that was labeled to a certain person or command. So, for the same user, there can be used multiple
 316 profiles, so in each one the software will be able to identify the specific trained commands only.

317 It means that the equipment would need to differentiate between two or more states at the same
 318 time. That configuration required more time to perform more training and required more effort to
 319 maintain the precision. Therefore, we opted to split in one profile per command. Therefore, the
 320 equipment would need to split between only two states making the ease to identify higher. Table 2
 321 presents a list of the main types of usability problems encountered and the number (N) of users who
 322 encountered those problems. The following subsections present a characterization of these problems.

Table 2. Categories of problems encountered.

Categories	Occurrences	N# of users
Training and execution of actions require a lot of user effort	20	15
Distractions affected training drastically	9	8
Different actions require different efforts	2	2
Command inaccuracy in relation to desired action	10	9
User shyness or anxiety hinder training	7	6

323 4.2.1. Training and execution of actions require significant user effort

324 Among the found problems during the testing, the most critical ones were related to a considerable
 325 effort during the training procedure. As it requires much attention, the repetitive tasks used to train
 326 the equipment could get cumbersome for at least half of the users. They complained that it was hard
 327 to focus enough, so the EEG performed precisely what they were willing to do.

328 For example, at the push statement that required the user to focus on pushing a virtual block to
 329 the bottom of the environment it was placed, the user needed to perform this mental command for
 330 seven seconds non-stop around four times, so the equipment could record the mental state at those
 331 seven seconds. This problem was mainly encountered due to reports after spending seven seconds
 332 training that they had used much concentration on it. Because for the first seven seconds of training,
 333 the block moved by itself to induce the user to understand better its mechanics. After that, with this
 334 option turned off, they realize how concentrated they need to be to push the block to the bottom and
 335 maintain it there during the training.

336 4.2.2. Distractions affected training drastically

337 Another problem encountered in the evaluations was the high level of attention needed. Even
 338 though numerous electrodes are available, compared to other base models, distractions still play a
 339 significant role in performance. During the operation, the users that distracted the most got the worst
 340 results or took longer to obtain a correct spot where the device knew the differences between neutral
 341 and non-neutral states. The way the EPOC+ works is by switching between trained phases. For
 342 example, if there are two trained states, the neutral one representing the absence of specific thoughts
 343 and the pushing one that makes a virtual block goes to the end of a corner. Therefore, the user is either
 344 neutral or pushing a block. Even though they are confounds, anything between those two states is
 345 assigned to one of the trained tasks. So, if the user performs the neutral state talking, thinking about
 346 something, or even distracting with ambient noises, the system is more inclined to associate that neural
 347 activity to a task that involves greater activation (push) instead of neutral that is associated with a
 348 more clear state of mind. Consequently, the participant will see the block moving when it was not
 349 supposed to and decrease the accuracy points perceived on the SAM ratings.

350 To prevent the user from distracting as much as possible, before starting the process, concentration
 351 is essential. Therefore, the participant was orientated not to pay attention to the test applicator and put
 352 away his cellphone.

353 According to Table 2, and regarding what was said about distractions during the test, in some
 354 cases it is possible to relate the inaccuracy to the lack of focus. However, problems with the connection
 355 between the user and the equipment sometimes happened and made the data from the electrical pulse
 356 more noisy or weak, causing the same problem.

357 4.2.3. Different actions require different efforts

358 As stated by Figure 6, the three actions that were chosen to compose the test required different
 359 amounts of training to obtain good precision. To reach that point of accuracy required, the metric
 360 Overall Skill Rating Figure 3 given by the Software was used. It indicated in percentage how precise
 361 the command was. In this context, the required precision level was above seventy per cent.

362 Until the user makes it to the precision mark, we observed that each test had a different mental
 363 workload. The Push command, even though it has the same range of training times, it has a slightly
 364 bigger median, and it has a more significant outlier associated with it. It can be justified by relating that
 365 this command was always the first, which means that the user's first contact with the workflow of the
 366 test can lead to some extra training. Therefore, the Lift command was started with more understanding
 367 and more user confidence, causing it to need less training to get a good precision range.

368 The command Smile did not have a performance metric to indicate how precise the action was.
 369 To identify the precision of it during the test, the user was asked to smile and come back to the neutral
 370 facial expression, and if it recognized at least three times straight, that command was considered
 371 precise for that user. As noticed in Figure 6, the median is significantly smaller than the previous
 372 commands, and the feeling of control associated with it was high in Figure 10.

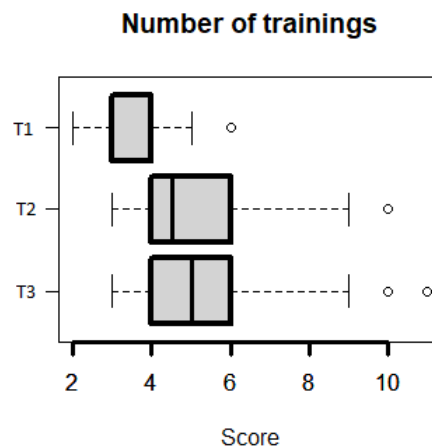


Figure 6. Number of training's required to get a good precision

373 4.2.4. Command inaccuracy in relation to desired action

374 Inaccuracy was a common problem found during training. Even with the minimum required
 375 precision to continue the test, one-third of the users dealt with a partial or a complete lack of accuracy.
 376 An attention lapse can cause that situation during the testing, the number of electrodes working (which
 377 could vary throughout the test), and the protocol break by acting differently from how it was trained.

378 For example, users who focused on the wall with their eyes opened to record the neutral state
 379 or decided to stay with the eyes closed to reduce one stimulus for the neutral state should reproduce
 380 this same state every time it was requested to stay at such state. However, when the user tried to see
 381 the block feedback while it was supposed to maintain its eyes closed, the feedback was not precise,

382 and the user was requested to restart the command performing exactly how he trained, leading to the
 383 perception of low precision.

384 4.2.5. User shyness or anxiety hinder training

385 Before the beginning of the test, some users demonstrated some level of shyness or anxiety.
 386 This phenomenon can be related to the lack of knowledge about EEG's and the disbelief in their
 387 performance. That event could happen before the test, as soon as the goal was explained and, less
 388 common, during it. Another factor that might create tension and, therefore, shyness was the usage of
 389 the camera to capture more information out of the test for further analysis.

390 To create an ideal circumstance for the user and avoid this situation, before any hardware setup, a
 391 conversation was carried to ensure that the videos would be seen exclusively by the testers. Another
 392 critical topic brought during this conversation was that the intention behind this test was strictly
 393 to evaluate the hardware accuracy and usability, showing that his/her performance would not be
 394 evaluated individually.

395 4.3. Emotional Reactions

396 Several emotions were identified during the test application and video analysis. The main ones
 397 depended on the circumstance where the neutral and excitement happened the most. In the beginning,
 398 a neutral expression was the most common. Users had doubts about the efficiency of what was being
 399 tested. As soon as the first command was successfully executed by the user, usually the push command,
 400 the frequent reaction of surprise and excitement were recorded. Since the predominance of positive
 401 test outcomes, both of these reactions were recurrent, and each time easier to identify the transition
 402 between them.

403 To measure the feelings and impressions throughout the test, users were requested to fill a form
 404 based on self-assessment manikin (SAM). This method contemplates a visual quiz based on images
 405 representing a scale. As shown in Figure 7, the first row contains an image scale that goes from a
 406 happy place to an apathetic one to represent the motivation dimension. The second row, represented
 407 by a sacred figure to a relaxed one, measures the satisfaction. The final question intends to measure the
 408 precision or how much control of its environment the user feels. According to Bradley [4], the SAM
 409 instrument represents an easy and quick way to measure effective responses after experiments and
 410 can be related to several benefits. Benefits include the reduced amount of data extracted and the ease
 411 to apply over populations like kids or elderly due to its lack of linguistic abilities.

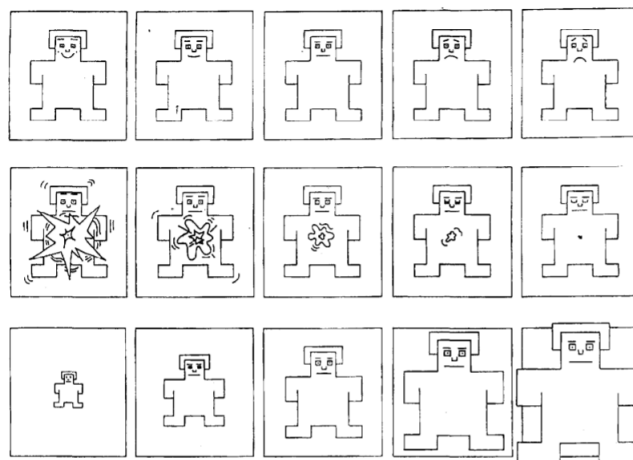


Figure 7. Self-Assessment Manikin test used to measure Motivation, Satisfaction and Feeling of control

412 The results are shown in Figure 8, Figure 9 and Figure 10 can demonstrate the median and the
 413 minimum or maximum values obtained after all the test procedures. For the Push command, it is

414 possible to see that the Motivation and Satisfaction indicators were higher than the Control Precision
415 one. This can be explained by the number of confounds encountered during testing. But, despite those
416 confounds, the median kept above the threshold.

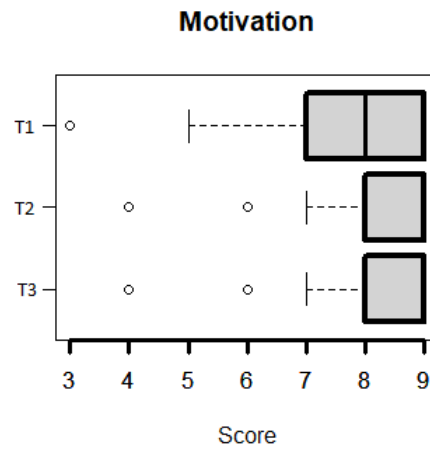


Figure 8. Motivation metric score

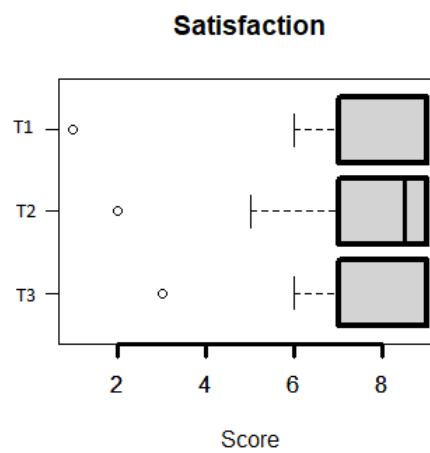


Figure 9. Satisfaction metric score



Figure 10. Feeling of control metric score

417 We performed related-samples Friedman's tests to verify if there were significant differences
 418 between the scores of motivation, satisfaction and sense of control for the commands smile, lift and
 419 push. No significant difference was found between the motivation scores for the commands push,
 420 lift and smile ($\chi_r^2 = 0.45$, $N=30$, $p\text{-value} = 0.79852$). No significant difference was found between the
 421 satisfaction scores for the commands push, lift and smile ($\chi_r^2 = 1.3167$, $N=30$, $p\text{-value} = 0.51771$). No
 422 significant difference was found between the feeling of control scores for the commands push, lift and
 423 smile ($\chi_r^2 = 2.6$, $N=30$, $p\text{-value} = 0.27253$).

424 According to the analysis made on the recorded videos of each training, there was considerable
 425 positive feedback. Most of them were related to the mental command portion of the training Figure
 426 11, instead of the facial expression, which might explain the higher score on motivation for those
 427 commands Figure 8.

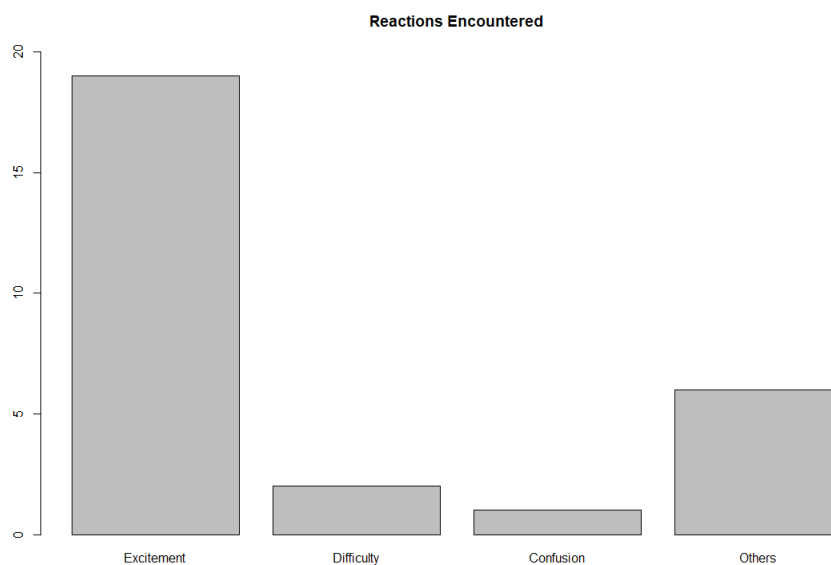


Figure 11. Emotional reactions encountered

428 In Figure 11, the emotions captured during the training were separated into four categories. The
 429 first one, called Excitement, represented positive feedback. These were accounted for when the user
 430 demonstrates statements or gestures such as Excitement, astonishment, or enthusiasm. The difficulty

431 referred to the category of discomfort, pain, or tiredness. The third one was assigned to confusion.
432 For example, the user could not perform was asked, needed further explanation, or demonstrated
433 a lack of comprehension during the test. The last one, Others, was related to confounding reports.
434 These reports included concentration deficits during the testing, requests to train an action again, or
435 precision complaints.

436 According to the graph shown in Figure 11, the most frequently captured emotions were positive.
437 Most of them were related to users being astonished by the successful mental command performed.
438 It can be explained by the fact that any of the participants have had no previous experience with
439 EEG technology. Yet not as common as the above mentioned, the E4 reactions were present in a
440 suitable recurrence, indicating that the experiment can be fragile to confounds like distractions and
441 concentration insufficiency at certain moments.

442 5. Discussion

443 The results indicate that implementing a brain-computer interface for the interaction with smart
444 homes is feasible due to the high accuracy found during the test. To support that statement, at Figure
445 10 can be noted a high level of acceptance from the users when it comes to precision which can be
446 correlated with Figure 8 that demonstrates that users kept motivated during the test. In that context,
447 those results yield a good non-invasive and non-intrusive environment. Also, the duration of the
448 whole test landed in between twelve and twenty-four minutes. Thirty users surpassed the studies
449 from Partha [24] and Luo [15] in the number of participants and also with none of the users being
450 familiarized with the technology like in [15].

451 Using non-static objects to train the subjects, unlike Partha [24] who displayed an image of a bulb,
452 yielded good metrics of motivation. That fact is observed in Figure 11, where excitement emotions
453 when the user saw the object moving due to its mental commands were frequent.

454 The methodological choices were constrained by having users with short hair due to the poor
455 contact with the scalp, caused by a thick layer between the electrodes and the skin. At Luo *et al.*'s [15]
456 study, there were women among the test users, and there were no records shown related to a poor
457 connection due to the hair layer. Also, it is beyond the scope of this study to test with disabled users.
458 Therefore, the generalizability of the results may be limited for that circle of people too.

459 Along with the procedures, the overall quality of the equipment decayed. Electrode fixation
460 points broke, forcing frequent maintenance and electrodes blackout. Moreover, that fixing process
461 involved leaving the electrode permanently attached to its headset base, making the whole equipment
462 even more fragile to minor impacts. Still, on the electrodes, the saline solution required to enhance the
463 connection caused over time a thick coat of rust, leading to bad connection problems that were only
464 solved when opened and grated.

465 Another complication, also found by Luo [15], was the delay between the equipment and the
466 computer. As the data is sent over Bluetooth, the distance between both parts and any blockage may
467 cause a delay on the commands. Moreover, as this study used interactive training, sometimes, that
468 delay created a more significant impact when the user was trying to lift or push the object, and it kept
469 still for a moment before it started moving. In this situation, the user sometimes tried to restart the
470 command, and as soon as he stopped thinking, the previous commands started reflecting and moving
471 the object. The whole situation can confuse the user and also decrease its sense of precision.

472 The training needed to be sliced into profiles that contained only one command because the usage
473 of one single profile that condensed all actions resulted in lower precision. Again, it would require
474 more time to practice and train commands and a higher level of focus, leading to a more invasive
475 procedure. By dividing the profiles, the software only demanded distinguishing between two phases,
476 the neutral and the command itself. Even though the neutral state training needed to be repeated at
477 every profile, the overall time still lower than the other approach, in which a big volume of training
478 per command was mandatory to reach the same accuracy.

479 As important as measuring the numeric feedback, the user experience and feelings are also
480 important. With these sorts of information, it is possible to understand not only if the model or the
481 equipment is accurate like Luo [15] and Partha [24] did, but also how the users feel about it throughout
482 the entire process. A big concern about EEG technology is finding a good ratio between precision and
483 the need to be invasive to achieve it. We can infer that the overall ease between facial expression and
484 mental commands is slightly lower with the obtained results. That is because the number of training
485 required to obtain a good precision is lower at facial expressions Figure 6. It might occur because
486 smiling, for example, does not require a mental overload as significant as mental commands. However,
487 the motivation associated with facial expression skewed more to the lower end of the score axis
488 than the Push or Lift commands. The positive feedback of excitement can explain that phenomenon
489 obtained multiple times when the user realized that his mental command controlled the environment
490 according to his thoughts Figure 11, something that lacked for the smiling training.

491 This study, used as subjects healthy and young people, but for users with some disability the
492 scenario could be different. Impairments, such as a stroke, can lead to blacked out areas of the brain.
493 Or even other types of limitations could lead to worse signal quality, therefore, this technology would
494 not be usable for some cases. Furthermore, some disabilities may cause difficulty on memorizing the
495 proxy commands, turning it into a complication that can lead to home control problems and even the
496 disability to control at all. For example, if a user has severe brain damage that has one of its side effects
497 as memory loss, a wrong command could lead to turning something off or leveling up the volume of a
498 TV too much. Also, the SAM applied to each participant, did not cover the difficulty of relating the
499 proxy to the command. Neither the test tried to identify the complexity of using all of them in a mixed
500 order to verify how well would the users perform when it comes to remembering each command.

501 6. Conclusion and Future Work

502 Intending to create a non-invasive and straightforward setup method that controls a smart
503 house for severely disabled people, the brain-computer interface using EPOC+ was adequate to
504 implement the prototype and to enable the usability evaluations. The research study provided relevant
505 contributions showing the usability benefits and limitations of employing an object-based abstraction
506 to perform mental commands with EEG-based interaction and the precision of such commands.

507 The main limitation that constrained the study was the feeble attachment between the electrode
508 and the scalp for users with thick hair. Also, the low quality of the fits for the electrodes, that delayed
509 the testing as a result of below twelve well-attached points on the head.

510 Regarding training, multiple actions combined at one profile resulted in more extended practice
511 and more significant focus, leading to a significantly larger mental overload. However, when separated
512 into one profile for each command, the training was faster and more accurate. Here, the usage of
513 interactive objects provides more motivation as the user realizes that he/she is controlling something.
514 Also, that concept helps the subject execute actions linked to a physical movement instead of an
515 abstract thought such as turning on a TV.

516 Based on these conclusions, future research should consider using more stable equipment and
517 ways to overcome physical limitations with the sensors. Other studies should also build upon the
518 findings from the present study to continue the design and perform user evaluations involving disabled
519 people.

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